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Mirjana Jovanić, ETRAN Zlatko Jarnević, ETRAN Marko Vujadinović, Academic Mind, Belgrade Aleksandar Rašković, Academic mind, Belgrade Boban Milijić, Academic mind, Belgrade This volume contains the papers presented at , 6th International Conference on Electrical, Electronic and Computing , (Ic)ETRAN 2019 in conjunction of ETRAN 63rd National Conference on Electrical, Electronic and Computing Engineering held on June 3-6, 2019 in Veliko Gradište.

There were 247 submissions. Each submission was reviewed by at least 1, and on the average 2, reviewers. The committee decided to accept papers as follows. Invited papers are included and presented as papers in Sessions.

During the Conferences were held three Special Sessions:

• Special Session dedicated to academician Rajko Tomović

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• Special Session: New Materials

Moderators:

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August 27, 2019 Belgrade Boris Loncar

Sinthesis and Characterization of Hydroxyapatite and Fluorapatite Powders

Željko Radovanović, Abdulmoneim Mohamed Kazuz, Predrag Vulić, Lidija Radovanović, Đorđe Veljović, Rada Petrović, Đorđe Janaćković

Abstract— The biomaterial powders of hydroxyapatite (HAp) and fluorapatite (FAp) were synthesized by a hydrothermal method. Powders were analyzed by energy-dispersive X-ray spectroscopy (EDS), field emission scanning electron microscopy (FESEM), and X-ray powder diffraction analysis (XRPD). EDS analysis shows the presence of non-stoichiometries FAp and HAp with molar ratio CA/P < 1.67. FESEM analysis of both powders indicates the presence of agglomerates of micrometric dimensions, while primary nanoparticles are rod-like. The Rietveld refinement of XRPD data showed that the single phase powders of FAp and HAp were synthesized. The results showed that obtained nanomaterials can be potentially applied in dentistry.

Index Terms—Biomaterial; Hydroxyapatite; Fluoroapatite; Nanoparticles; Rietveld refinement.

I. INTRODUCTION

A new trend in the treatment of teeth is the application of material that would fill the cavity after removal of damaged dental tissue and also remineralize the surrounding tissue. The appropriate material could be a hydroxyapatite (HAp) as well as fluorapatite (FAp). Synthetic HAp, $Ca_5(PO_4)_3(OH)$, is similar to the inorganic part of bones and the dentine of teeth. It is biocompatible, bioactive, nontoxic, and osteoconductive [1, 2]. Replacement of the OH⁻ groups in HAp with F⁻ gives FAp, an implant material with better hardness, greater stability, less solubility and better antimicrobial effect than HAp [1].

Taheri *et al.* [3] synthesized the FAp by hydrothermal method at different pH values and temperatures. They found that the pH value of hydrothermal solution is more significant

Željko Radovanović is with the Innovation Center of the Faculty of Technology and Metallurgy, University of Belgrade, Karnegijeva 4, 11120 Belgrade, Serbia (e-mail: zradovanovic@tmf.bg.ac.rs).

Abdulmoneim Mohamed Kazuz is with the Faculty of Technology and Metallurgy, University of Belgrade, Karnegijeva 4, 11120 Belgrade, Serbia (e-mail: abdulmohamedabdul520@gmail.com).

Predrag Vulić is with the Faculty of Mining And Geology, University of Belgrade, Đušina 4, 11000 Belgrade, Serbia (e-mail: predrag.vulic@rgf.bg.ac.rs).

Lidija Radovanović is with the Innovation Center of the Faculty of Technology and Metallurgy, University of Belgrade, Karnegijeva 4, 11120 Belgrade, Serbia (e-mail: lradovanovic@tmf.bg.ac.rs).

Dorđe Veljović is with the Faculty of Technology and Metallurgy, University of Belgrade, Karnegijeva 4, 11120 Belgrade, Serbia (e-mail: djveljovic@tmf.bg.ac.rs).

Rada Petrović is with the Faculty of Technology and Metallurgy, University of Belgrade, Karnegijeva 4, 11120 Belgrade, Serbia (e-mail: radaab@tmf.bg.ac.rs).

Dorde Janaćković is with the Faculty of Technology and Metallurgy, University of Belgrade, Karnegijeva 4, 11120 Belgrade, Serbia (e-mail: nht@tmf.bg.ac.rs).

factor than temperature in terms of shape and dimension of the synthesized FAp. Ge et al. [4] obtained FAp after heat treatment at 600 °C in a water vapor environment for 3 h started from the as-deposited amorphous fluoridated calcium phosphate. They revealed that FAp had significantly better antibacterial activity than HAp. Stanić et al. [5] synthesized FAp powders by neutralization method. They found that the antimicrobial activity of the samples increases with the increase of concentration of F-and decrease of pH value of saline solution. Zhao et al. [6] have shown that by the solution combustion method is possible to obtain single phase FAp and HAp starting from inexpensive raw materials and applying relatively simple preparation process and low-cost experimental installation.

The aim of this study was to synthesize the pure nanosized powders of FAp and HAp and investigate the properties of these materials. For this purpose, modified hydrothermal synthesis was applied.

II. MATERIALS AND METHOD

FAp and HAp powders were synthesized by a previously described modified hydrothermal method [7–10]. Pure HAp was synthesized from stoichiometric quantities of the chemicals: NaH₂PO₄·2H₂O (VWR Prolabo, 99.8%), NH₄OH (Zorka Pharma, p. a.) and Ca(NO₃)₂·2H₂O (Roth, \geq 98%). In the synthesis of FAp, beside aforementioned chemicals, NaF (Riedel de Haen, 99%), were also used. Synthesis was performed with a constant molar ratio Ca/P = 1.67. After dissolution of the chemicals in 2 L of distilled water, the dish with the solution was inserted into an autoclave, previously filled with the 1.5 L of distilled water. The solution was heated at 160 °C for 3 h. After slow cooling, the obtained suspension was filtered, and the residue was washed with distilled water and dried at 105 °C for 4 h.

Energy-dispersive X-ray spectroscopy (EDS) of the powders was performed on a Jeol JSM 5800 SEM with a SiLi X-Ray detector (Oxford Link Isis series 300, UK).

The morphologies of the powders were observed by Tescan Mira 3 XMU field emission scanning electron microscopy (FESEM). Before analysis, the powders were coated with Au using a Polaron SC502 sputter coater. The particle size distribution was determined and presented using Mira software and Microsoft Excel programme, respectively.

The X-ray powder diffraction (XRPD) measurements were performed on a Rigaku SmartLab diffractometer using Cu $K\alpha$ radiation, at 40 KV and 30 MA, in Bragg–Brentano geometry. Diffraction data were collected in the range $5^{\circ} < 2\theta < 120^{\circ}$ (scan speed: 1° min⁻¹, step width: 0.01° 2θ) at room temperature.

III. MAIN RESULTS

The atomic % of O, Ca, P and F were determined from the results of EDS analysis (Table I). This analysis shows the presence of non-stoichiometric HAp and FAp with molar ratio Ca/P < 1.67, which means that in both cases Ca-deficient apatite is synthesized.

 TABLE I

 EDS results for FAp and HAp powders.

Atomic %	Powder	
	НАр	FAp
0	72.71±0.23	66.16±1.06
F	_	5.00±0.58
Р	11.53±0.05	11.58±0.27
Ca	15.75±0.20	17.26±0.69
Ca/P	1.37	1.49

The FESEM micrographs of the hydrothermally obtained HAp and FAp powders are shown in Fig. 1. Both powders consist of rod-like nanosized particles with average particle size of 87 ± 17 nm for HAp and 87 ± 20 nm for FAp. Also, the particle size distribution (Fig. 2.) are very similar and more than 60 % of particles are in the range of 70–90 nm for both powders. The particles form the agglomerates of micrometric dimensions. In the case of HAp, the agglomeration is more pronounced.



Fig. 1. FESEM micrographs of the HAp and FAp powders.



TABLE II Crystallographic and Rietveld refinement parameters of HAP and FAP

AND FAP.			
Phase	НАр	FAp	
Crystal system	hexagonal	hexagonal	
Space group	$P6_{3}/c$	P6 ₃ /c	
a [Å]	9.4205(1)	9.3760(1)	
<i>c</i> [Å]	6.88151(9)	6.88276(9)	
V [Å ³]	528.9(1)	524.0(1)	
Crystallite size	346(1)	330(1)	
[Å]	[-0.356, 0.935, 0]	[0.356, -0.935, 0]	
Crystallite size	346(1)	330(1)	
[Å]	[0.935, 0.356, 0]	[0.935, -0.356, 0]	
Crystallite size [Å]	886(9) [0, 0, 1]	983(1) [0, 0, 1]	
Strain [%]	0.096(2)	0.105(1)	
<i>R</i> _{wp} [%]	4.87	4.92	
<i>R</i> _p [%]	3.76	3.82	
<i>R</i> e [%]	3.92	3.92	
χ^2	1.5414	1.5744	
S	1.2451	1.2548	
Maximum shift/e.s.d.	0.081	0.022	



Fig. 3. Rietveld refinement (up) and crystal packing diagram in *ab* plane (down) of HAp.

XRPD patterns of HAp and FAp (Figs. 3 and 4, respectively) are very similar, but the peaks in the XRPD pattern of FAp are mildly shifting to higher values of 2θ angles indicating that unit cell of FAp is smaller.

The structures of HAP and FAp are presented in Figs. 3 and 4, respectively. The both structures crystallize in the hexagonal space group P6₃/*c*, with two formula units Ca₅(PO₄)₃OH per unit cell, for HAp and with two formula units Ca₅(PO₄)₃F for FAp. The lattice parameters for both structures are presented in Table II, from which it can be seen that unit cell of FAp is slightly smaller because of the substitution of OH⁻ group with F atom. Also, the crystallites of HAp and FAp are more elongated along the *c* axis (Table II) which is in accordance with rod–like morphology of particles observed by FESEM.

Rietveld refinement showed that there is no deficiency of Ca atoms in the structures of HAp and FAp, so the ratio Ca/P < 1.67 obtained by EDS analysis can be attributed to the errors of this method.





Fig. 4. Rietveld refinement (up) and crystal packing diagram in *ab* plane (down) of FAp.

TABLE III Selected bond lengths (Å)for HAp and FAp		
НАр	FAp	
Ca1-O1 2.401	Ca1-O1 2.392	
Ca1-O2 2.452	Ca1–O2 2.449	
Ca1-O3 2.836	Ca1-O3 2.820	
Ca2–O1 2.703 Ca2–O2 2.365 Ca2–O3 2.329	Ca2–O1 2.689 Ca2–O2 2.367 Ca2–O3 2.338	
Ca2- O4 2.396	Ca2-F1 2.312	
P1-O2 1.536 P1-O1 1.535	P1-O1 1.537 P1-O2 1.542	

The selected bond lengths for HAp and FAp are listed in Table III. The Ca2–F1 bond length in FAp is shorter than Ca2–O4 (O4 is from the OH^- group) bond length in HAp, which can possibly be the reason for smaller unit cell of FAp.

P1-O3 1.537

P1-O3 1.542

IV. CONCLUSION

The pure, rod-like nanoparticles of HAp and FAp, suitable for application in teeth treatment, have been prepared by simple hydrothermal synthesis. Due to the presence of very small particles, using these materials in filling the tooth's canal is more preferable in comparison with similar materials but with microsized particles.

The future investigations will be oriented towards the synthesis of nanosized Ca-deficient HAp and FAp powders that could be doped further with different metal ions $(Mg^{2+}, Si^{4+}, Na^+, Cu^{2+}, etc.)$. Also, the composite materials will be prepared by mixing of the appropriate ratio of HAp and FAp and their potential use as dental material will be examined.

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