





## Article

# Influence of Novel SrTiO<sub>3</sub>/MnO<sub>2</sub> Hybrid Nanoparticles on Poly(methyl methacrylate) Thermal and Mechanical Behavior

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**Abstract:** While dental poly methyl methacrylate (PMMA) possesses distinctive qualities such as ease of fabrication, cost-effectiveness, and favorable physical and mechanical properties, these attributes alone are inadequate to impart the necessary impact strength and hardness. Consequently, pure PMMA is less suitable for dental applications. This research focused on the incorporation of Strontium titanate (SrTiO<sub>3</sub>-STO) and hybrid filler STO/Manganese oxide (MnO<sub>2</sub>) to improve impact resistance and hardness. The potential of STO in reinforcing PMMA is poorly investigated, while hybrid filler STO/MnO<sub>2</sub> has not been presented yet. Differential scanning calorimetry is conducted in order to investigate the agglomeration influence on the PMMA glass transition temperature (T<sub>g</sub>), as well as the leaching of residual monomer and volatile additives that could pose a threat to human health. It has been determined that agglomeration with 1 wt% loading had no influence on T<sub>g</sub>, while the first scan revealed differences in evaporation of small molecules, in favor of composite PMMA-STO/MnO<sub>2</sub>, which showed the trapping potential of volatiles. Investigations of mechanical properties have revealed the significant influence of hybrid STO/MnO<sub>2</sub> filler on microhardness and total absorbed impact energy, which were increased by 89.9% and 145.4%, respectively. Results presented in this study revealed the reinforcing potential of hybrid nanoparticles that could find application in other polymers as well.

**Keywords:** nanoparticles; SrTiO<sub>3</sub>/MnO<sub>2</sub>; PMMA composite; mechanical properties



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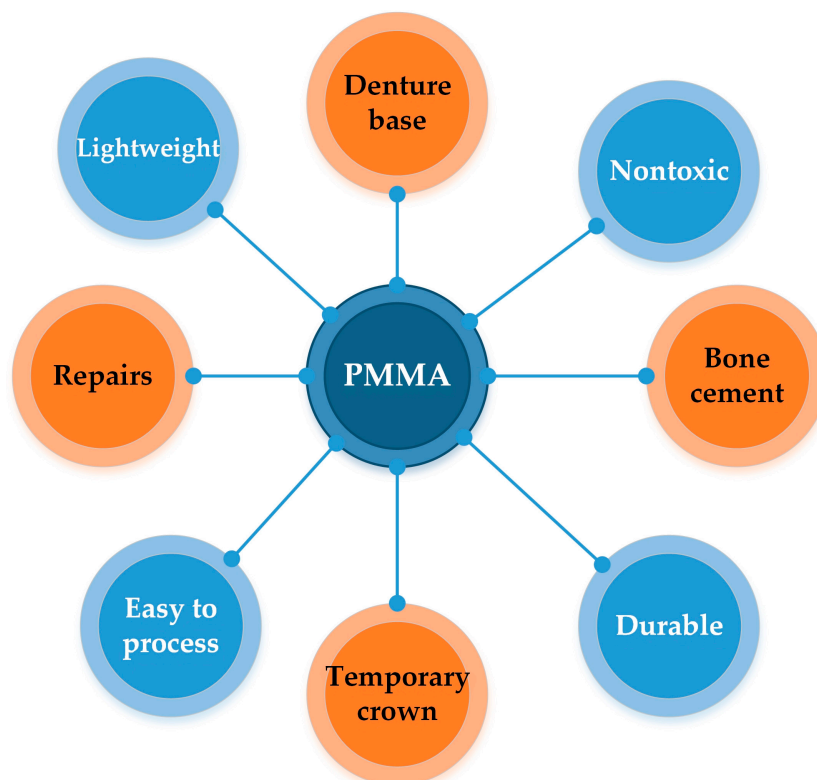
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## 1. Introduction

Various polymers have widespread use in the field of dentistry, from bone cement materials or repairs to drug delivery [1–3]. Among these, poly methyl methacrylate (PMMA) stands out as a versatile polymer extensively utilized for crafting orthodontic retainers, dentures, and repairs, as well as artificial teeth [4–6]. Scheme 1 illustrates an array of advantages and applications of PMMA. Years of research and practical application have established that PMMA provides durability, nontoxicity, ease of processing, and hence, economic viability, as well as high biocompatibility [7].

However, along with the noted advantages, there are important drawbacks in mechanical properties that hinder widespread PMMA application [8,9], leading to studies on the improvement of mechanical strength, toughness, impact resistance, and hardness [10]. One of the approaches to enhance the mechanical performance of PMMA is by introducing fillers that can tune both, mechanical and functional properties. Numerous studies have presented improvements in targeted PMMA properties materials by incorporating fibers or

nanoparticles [11–17]. Among the versatile selection of nanoparticles, silica ( $\text{SiO}_2$ ), alumina ( $\text{Al}_2\text{O}_3$ ), titania ( $\text{TiO}_2$ ), and zirconia ( $\text{ZrO}_2$ ) are the most investigated as reinforcements for PMMA, due to their mechanical and antibacterial potential [17–22]. These particles are also known for their ability to form various surface architectures at microscopic and nanoscopic levels, which further enables control of various functional properties [23]. Vojdani et al. improved hardness by 13% with the addition of 5 wt% of alumina to PMMA [24]. Hata et al. reported a more than 100% increase in hardness with 23% of nanoporous silica [25]. On the other side, Alhotan et al. achieved only a 10% hardness increase with 7% of nano-zirconia [26]. Furthermore, Gad et al. discovered that, although  $\text{ZrO}_2$  increases flexural properties, it also decreases the impact strength of PMMA [27].



**Scheme 1.** Advantages and applications of PMMA in dentistry.

In order to enhance mechanical properties and overcome challenges involving the enhancement of one property at the expense of another, research has been focused on the hybrid concept i.e., combinations of different particles, nanotubes, or fibers, with the aim of achieving a synergistic effect between the reinforcements. Recently, Naznin et al. increased the tensile strength of PMMA by 329% by incorporating graphene oxide and mesoporous micro-silica ( $\text{SiO}_2$ ) [28]. Chen et al. incorporated nanoparticles of  $\text{TiO}_2$  and micro poly(ether ether ketone) (PEEK) in order to increase the bending strength and flexural modulus of PMMA. With 1 wt% of  $\text{TiO}_2$  and PEEK, both flexural strength and modulus increased by 10% compared to control PMMA [29]. Alqahtani et al. reported that with a 10% load of Zirconia-Yttria ( $\text{ZrO}_2\text{-Y}_2\text{O}_3$ ) hardness of PMMA was increased 4.5 times, while flexural strength showed an increase of 7 times [30]. The same group incorporated hexagonal boron nitride (h-BN) in PMMA, varying concentration and particle size [31]. They reported a 2.7 times increase in hardness with 5 wt% of h-BN loading. By using hybrid reinforcement  $\text{Al}_2\text{O}_3/\text{TiO}_2$  nanoparticles, Nabhan et al. increased the fracture toughness of PMMA by 10% with only 1.6 wt% of the filler [32]. According to Wu et al., with 9% of nano hydroxyapatite and 12.5% nano alumina, a 40% increase in fracture toughness could be achieved [33]. Obviously, applying multiple reinforcements within the same polymer matrix brings more benefits than using individual fillers. Additionally, hybrid particles can

enable the enhancement of biocompatibility and bioactivity, as shown by Beketova et al. in the investigation of the  $ZrO_2$ - $Y_2O_3$  system [34].

Numerous ongoing studies are focused on processing PMMA-based nanocomposites, where there are still many challenges to improving mechanical properties without disrupting biocompatibility or cost-effectiveness. A perovskite-structured oxide called strontium titanate ( $SrTiO_3$ -STO) is known for its excellent piezoelectric, dielectric, and thermoelectric properties, as well as photocatalytic activity [35–37]. However, it has also been recognized in medicine, due to biocompatibility and bioactivity, as an osteogenesis promoter; furthermore, STO exhibits antibacterial activity, which makes it a valuable material for implants [38–40]. Si et al. showed that STO promotes the improvement of tribological properties, as well as the antibacterial activity when applied on titanium-based implants [41]. The potential of nanoparticle STO application in dental materials has still been limited to implant coatings, although it could offer advantages in other fields of medicine, as it has exceptional mechanical properties, such as high Young's modulus, compressive strength, and hardness [36,42].

Another oxide that could be valuable for tuning PMMA properties is manganese oxide ( $MnO_2$ ), due to its nontoxicity, antibacterial activity, resistance to acids, and low cost [43–46]. Although  $MnO_2$  has mostly been researched for its catalytic activity, its use in medicine and environmental protection was recently emphasized as well [47,48]. There are very few studies on the mechanical benefits of the incorporation of  $MnO_2$  in polymer matrices. However, Balguri et al. recently reported that with only 0.1 wt% of  $MnO_2$ , the impact strength of epoxy was improved by 35% [49]. Zhao et al. incorporated  $MnO_2$  in polyvinylidene fluoride (PVDF) in order to enhance the piezoelectric and mechanical performance of composites [50]. With 1.5 wt% loading of  $MnO_2$ , Young's modulus was increased by 75%, showing the reinforcing potential of this oxide.

While there is obvious potential for STO and  $MnO_2$  nanoparticle-reinforced PMMA, there is a lack of research investigating the influence of these ceramic materials on the mechanical properties of PMMA, with a special emphasis on impact resistance and hardness, which are crucial for dental materials. This research focuses on the mechanical performance of PMMA reinforced with STO and hybrid STO/ $MnO_2$  nanoparticles. Obtained composites showed significant improvement in Young's modulus of elasticity, hardness, and impact resistance.

## 2. Materials and Methods

### 2.1. Materials

$SrTiO_3$ , nanopowder and  $MnO_2$  were purchased from Sigma–Aldrich. PMMA was purchased from AKRILAT, Serbia. Commercial dental acrylic resin is made of two components system, liquid and powder. The liquid part contains methyl metacrylate (MMA)—monomer and inhibitor, while the powder contains PMMA, initiator, plasticizer, and pigments. Upon mixture of the two parts, the initiator neutralizes the effect of the inhibitor allowing the polymerization reaction to start.

### 2.2. Preparation of Samples

$SrTiO_3$ / $MnO_2$  (STO/ $MnO_2$ ) nanoparticles were prepared by milling for 30 min and heating for 2 h at 1000 °C, with a 5 °C/min heating rate, in  $N_2$  atmosphere. The molar ratio  $SrTiO_3$ : $MnO_2$  was 5:1.

Composites were prepared in three steps:

- Particles were placed in a liquid part containing MMA, and mixed on a magnetic stirrer, followed by ultrasonic homogenization.
- The liquid part with STO/ $MnO_2$  nanoparticles was mixed with powder in a volumetric ratio of 35/100, in accordance with the manufacturer's instructions.
- The mixture was poured into a mold and left for 24 h at room temperature.

The overall concentration of nanoparticles was 1 wt%. Samples were labeled as follows: PMMA, PMMA-STO, and PMMA-STO/MnO<sub>2</sub>.

### 2.3. Characterization of Samples

For morphological analysis of samples, field emission scanning electron microscopy (FESEM) was utilized with Tescan Mira 3 instruments (Brno, Czech Republic), where gold was sputtered prior to imaging. Particle size was determined by analysis of three FESEM images using the software *Image-Pro Plus 6.0* (Rockville, MD, USA). Structural analysis of STO/MnO<sub>2</sub> nanoparticles was performed using an X-ray diffractometer (XRD) Ultima IV, Rigaku (Tokyo, Japan). The measurement was performed using Cu K $\alpha$  radiation, with the following measurement parameters: 2 $\theta$  angle range from 20° to 80°, speed 10° min<sup>-1</sup>, step scan 0.02°. For the structural analysis of PMMA and composites, Fourier transform infrared spectroscopy (FTIR) was performed using a Thermo Scientific Nicolet iS10 spectrometer (Hartmann & Braun, MB-series, Bockenheim, Germany), in the range from 4000 to 500 cm<sup>-1</sup>, with a resolution of 4 cm<sup>-1</sup>. Differential scanning calorimetry (DSC) was performed on Shimadzu DSC-60Plus (Kyoto, Japan). The sample weight was 6 ± 0.5 mg. Initially, the samples underwent heating from 24 °C to 160 °C, with a heating rate of 10 °C/min in the presence of a nitrogen gas flow (50 mL/min). Subsequently, the second heating cycle was conducted under identical conditions. The data from the second heating cycle were used for the determination of T<sub>g</sub>. Tensile test of pure PMMA and composites was obtained by texture analyzer Shimadzu EZ Test LX, in accordance with ISO 527-2 standard (Kyoto, Japan) for plastics. The device was equipped with a 500 N load cell, applied strain rate was 10 mm/min. Cross-section area and gauge length were measured before each test. *Trapezium 1.5.2* software (Duisburg, Germany) by Shimadzu was used for the calculation of modulus of elasticity and tensile strength. All of the measurements were performed at room temperature. Microindentation testing was performed on the same device, with the following parameters set: 500 N load cell, a spherical indenter of 4 mm diameter, indentation rate of 0.25 N/s. The maximum load of 5 N was kept for 20 s, after which was decreased at the same rate of 0.25 N/s. The output results were force, time, and relative position of the indenter. Measurements were performed on three points for each sample, to reduce the influence of possible inhomogeneity. High-speed puncture impact testing machine HYDROSHOT HITS-P10, Shimadzu (Kyoto, Japan), was used for the investigation of nanoparticle influence on the impact resistance of PMMA. Absorbed energy (total absorbed energy-E<sub>tot</sub> and energy at maximum load-E<sub>fmax</sub>) values were calculated automatically from the load-time diagram. The diameter of the striker was 12.7 mm, with a hemispherical head; the set impact force was 10 kN, and impact velocity and depth were 0.15 m/s and 1 mm, respectively. For impact testing, samples had dimensions 6 × 6 × 3 cm<sup>3</sup>. Each measurement was performed on three samples, with the average values noted in the results.

## 3. Results and Discussion

### 3.1. FESEM of STO/MnO<sub>2</sub> Nanoparticles

Figure 1a shows an FESEM image of prepared STO/MnO<sub>2</sub> particles. As can be seen, spherical-shaped nanoparticles formed aggregates due to electrostatic forces, coming from STO that is dominant in our sample [51]. Image analysis showed that the average particle diameter was around 48 nm, with a modal value of approximately 35 nm. Distribution of particle size (Figure 1b) revealed that more than 60% of the particles had diameters below 50 nm and 93% were below 100 nm, which suggests a successful synthesis of nanoparticles that could contribute to the mechanical reinforcement of PMMA.

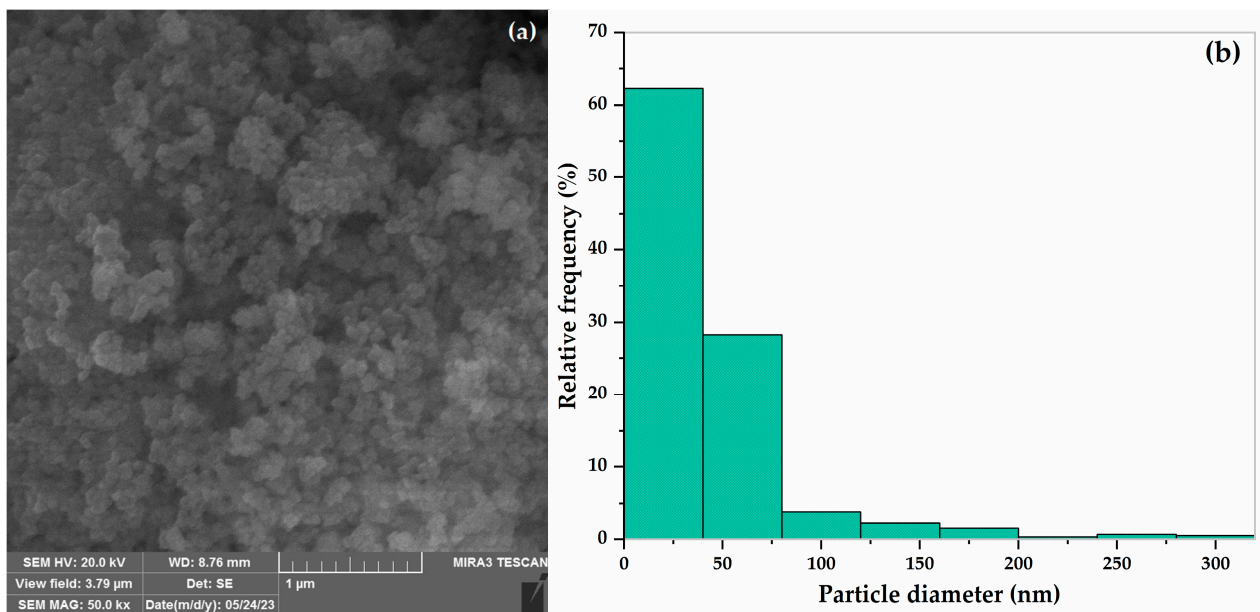


Figure 1. (a) FESEM of STO/MnO<sub>2</sub> (b) Particle size distribution.

### 3.2. XRD of STO/MnO<sub>2</sub> Nanoparticles

Figure 2 shows the diffraction pattern of STO/MnO<sub>2</sub> particles. The strongest peaks observed in the STO/MnO<sub>2</sub> are detected at angular positions of 32.4, 40.0, 46.3, 57.8, 67.8, and 77.0°. These peaks are attributed to the crystallographic planes of STO possessing cubic symmetry, specifically corresponding to (110), (111), (200), (211), (220), and (311) orientations [35,52]. Diffraction originating from MnO<sub>2</sub> also shows four peaks at 28.8, 37.2°, 56.7° and 72.4° attributed to the (110), (101), (211) and (112) planes of  $\beta$ -MnO<sub>2</sub> polycrystalline nanoparticles consisting of pure single tetragonal phase system [53,54]. The peak at 22.7° probably belongs to orthorhombic  $\gamma$ -MnO<sub>2</sub>, which also exhibits peaks at 37.2°, 56.2, and 67.8° that overlap with  $\beta$ -MnO<sub>2</sub> and STO [55–57]. Residual SrCO<sub>3</sub> in commercial STO was detected at 25.1°, corresponding to the (111) plane, which remained present even after the heat treatment at 1000 °C [58].

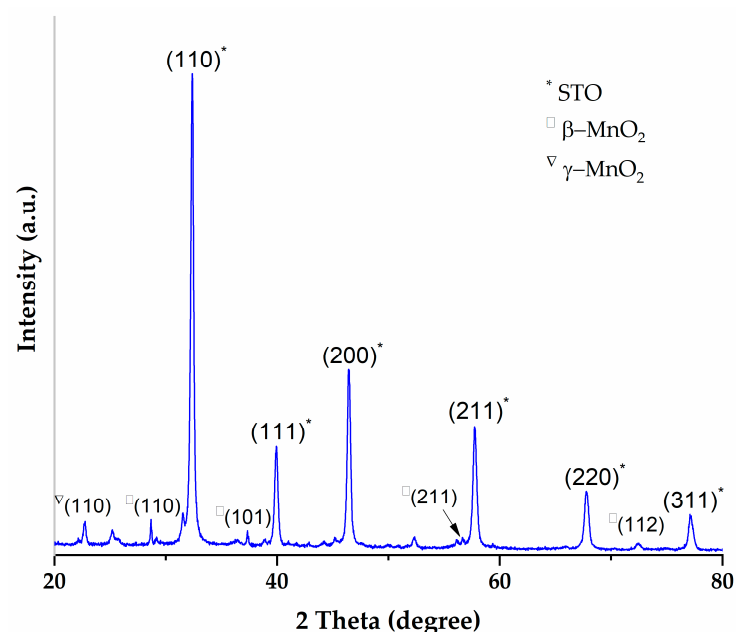


Figure 2. XRD of SrTiO<sub>3</sub>/MnO<sub>2</sub> particles.

Results obtained by XRD analysis indicate that synthesized nanoparticles were STO/MnO<sub>2</sub> composites, with crystal lattices intact. In this manner, properties of the separate compound should be retained and the possibility of synergistic effect enhanced. Furthermore, two phases of MnO<sub>2</sub> were identified,  $\beta$ -MnO<sub>2</sub> and  $\gamma$ -MnO<sub>2</sub>, as a consequence of high-temperature treatment.

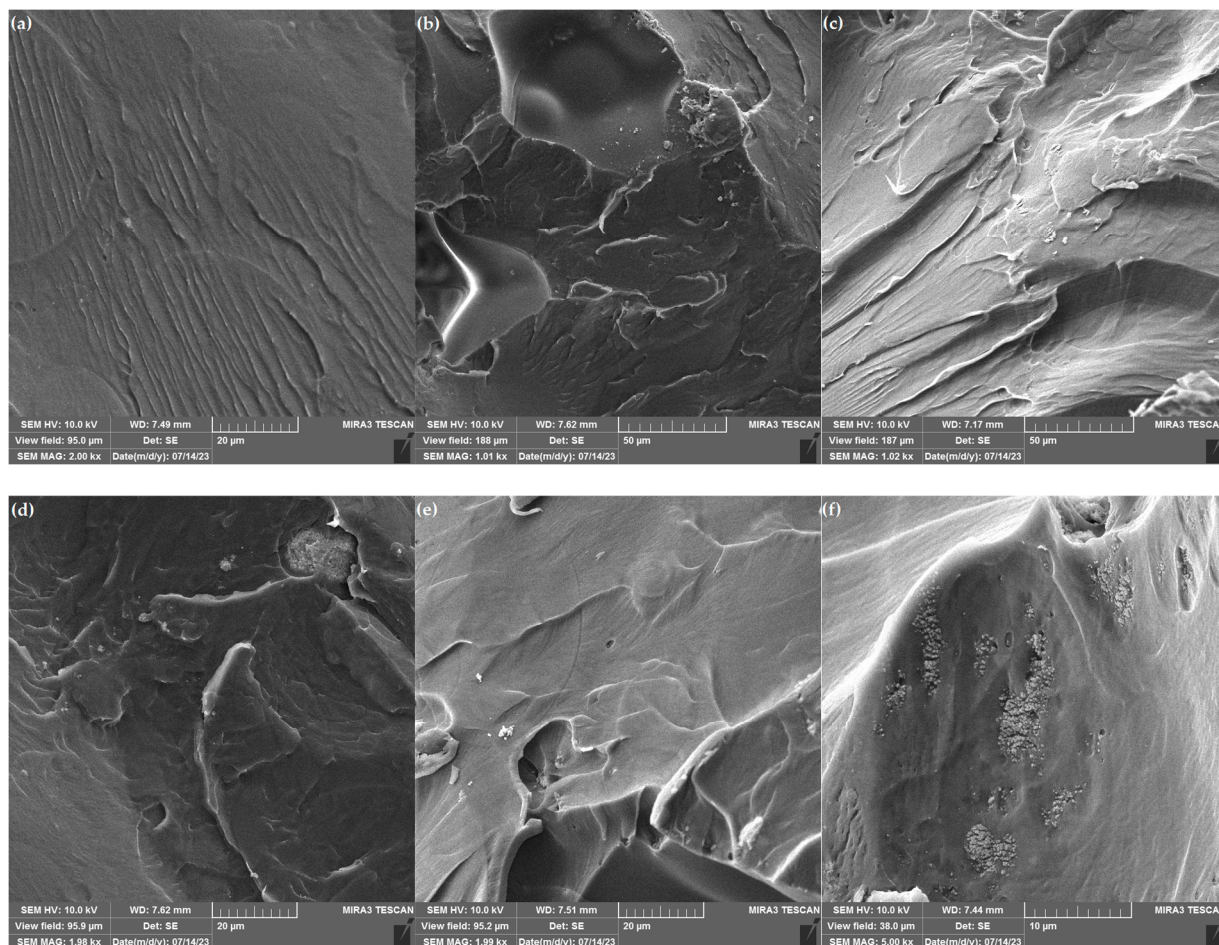
### 3.3. FESEM of PMMA and Composites

Morphological analysis of the fracture site was performed on FESEM images presented in Figure 3. Particle-reinforcing effects in composites play a crucial role in determining their mechanical properties, especially at the fracture site [59,60]. During polymerization, various inter-constituent changes occur, such as twisting, bending, and flexing, which influence particle-polymer interfacial surface and consequently, mechanical properties, such as toughness and elastic behavior [61]. The following crucial toughening mechanisms can be identified in FESEM images [59]:

- **Crack Bridging:** Particles can bridge microcracks that form within the composite matrix. As a crack attempts to propagate, it encounters bridges, which resist further crack growth. The bridging mechanism increases the energy required for crack propagation enhancing the composite's fracture resistance.
- **Crack Deflection:** Particles can cause cracks to change direction when they encounter the particle-matrix interface. This deflection reduces the effective crack length, increasing the composite's resistance to fracture and improving its toughness.
- **Crack tip pinning:** As the crack propagates and encounters a pinning point, it experiences local resistance. This resistance arises due to the additional energy required to deform the material or overcome the obstacles presented by the pinning point. The energy required to deform the material around the pinning point, or to move the crack past the obstacle, is dissipated as heat. This energy dissipation contributes to the overall toughness of the material.

Comparison of PMMA morphology with composites clearly shows the reinforcing effect of both STO and STO/MnO<sub>2</sub> particles. Pure PMMA surface (Figure 3a) shows a typical brittle fracture, with smooth fracture surface and river-like patterns, where plastic deformation plays a key role in fracture resistance [62]. On the other hand, both composites, PMMA-STO and PMMA-STO/MnO<sub>2</sub> (Figure 3b,c), show different toughening mechanisms. The fracture surface of both PMMA-STO and PMMA-STO/MnO<sub>2</sub> showed higher roughness compared to PMMA, which is directly connected to a reinforcement in the material. The inclusion of the filler in the matrix microstructure restricts dislocation movement during loading, thereby enhancing the strength and modulus of the composites [32]. Formation of aggregates was observed, which also served as a reinforcement-inducing crack-pinning mechanism [63]. Strong plastic deformation also reveals increased fracture resistance. The dominant toughening mechanism was crack-pinning in both composites, whereas pure STO particles formed large aggregates that participated in crack arrest through plastic void formation as well [64]. On the fracture surface of PMMA-STO/MnO<sub>2</sub>, small aggregates were formed, indicating better dispersion of hybrid nanoparticles in composite, presumably due to the formation of a larger interfacial surface [61].

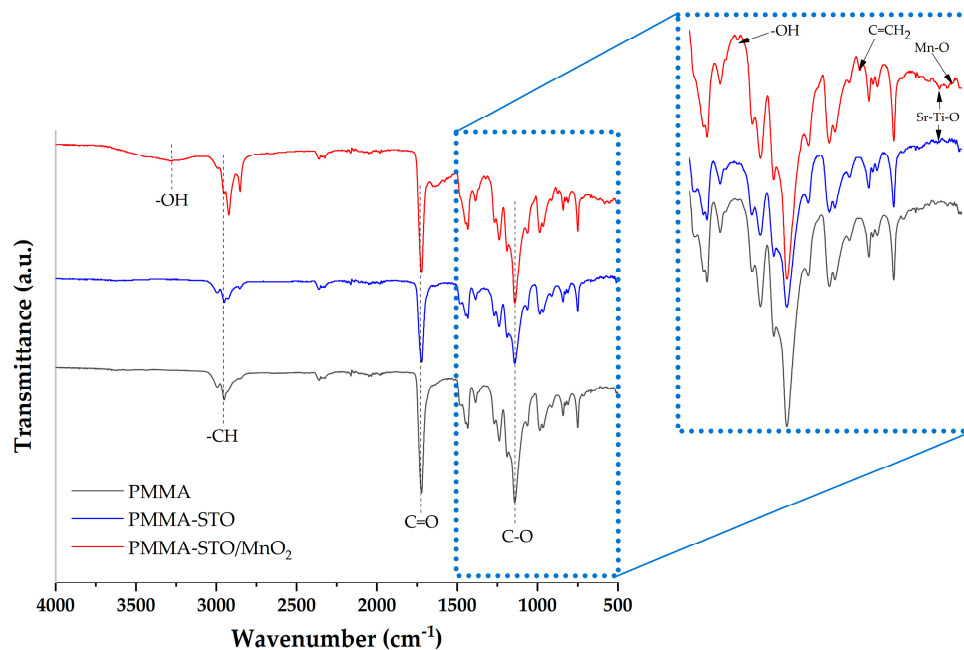
By increasing the magnification from 1000 $\times$  to 2000 $\times$  (Figure 3d,e), an obvious difference in agglomeration was observed. While STO/MnO<sub>2</sub> showed some uniformity in agglomerate size, pure STO showed a wide range of sizes, from around 1  $\mu$ m to 20  $\mu$ m. This could be the consequence of weaker van der Waals forces in hybrid nanoparticles compared to pure STO. However, in PMMA-STO/MnO<sub>2</sub>, a group of smaller agglomerates surrounded by a polymer matrix was found with 5000 $\times$  magnification, which caused significant plastic deformation and void formation as a toughening mechanism. Based on FESEM analysis, it was expected that both STO and PMMA-STO/MnO<sub>2</sub> nanoparticles would contribute to the reinforcement of the matrix material.



**Figure 3.** FESEM images of (a) PMMA (2000 $\times$  magnification); (b) PMMA-STO (1000 $\times$  magnification); (c) PMMA-STO/MnO<sub>2</sub> (1000 $\times$  magnification); (d) PMMA-STO (2000 $\times$  magnification); (e) PMMA-STO/MnO<sub>2</sub> (2000 $\times$  magnification); (f) PMMA-STO/MnO<sub>2</sub> (5000 $\times$  magnification).

### 3.4. FTIR of PMMA and Composites

In Figure 4, the infrared spectra of the pristine PMMA, PMMA-STO, and PMMA-STO/MnO<sub>2</sub> are presented. In order to emphasize the differences between spectra, especially in the fingerprint region, region 1500–500 cm<sup>-1</sup> was enlarged in Figure 4. The asymmetric stretching of C-H bonds, present in -CH<sub>3</sub> manifests itself at 2995 cm<sup>-1</sup> in all spectra [65]. At 2925 and 2856 cm<sup>-1</sup>, asymmetric and symmetric C-H stretch in -CH<sub>2</sub> was observed, respectively. Notably, the stretching vibration of the ester group's C=O bond is prominently evident at approximately 1721 cm<sup>-1</sup> [66]. The strong peak at 1430 cm<sup>-1</sup> originates from the asymmetric bending vibrations of the C-CH<sub>3</sub>. Two sets of doublet bands, one at 1267 and 1241 cm<sup>-1</sup> and the other at 1143 and 1183 cm<sup>-1</sup> can be attributed to the C-O stretching vibrations within the ester groups [67,68]. Out-of-plane -CH bending is present in the region from 900 to 720 cm<sup>-1</sup> [62,69]. In the spectrum of PMMA-STO/MnO<sub>2</sub>, a minor band at 875 cm<sup>-1</sup> could be associated with the bending of CH from C=CH<sub>2</sub> in residual monomer methyl methacrylate, indicating that agglomerates act as interceptors for monomer during polymerization reaction. Furthermore, peaks visible at 3277 cm<sup>-1</sup> originate from stretching vibrations of hydroxyl groups related to the STO/MnO<sub>2</sub> nanoparticles [55]. Bands at 1637 cm<sup>-1</sup> and 1320 cm<sup>-1</sup> come from -OH bending. The most prominent peaks in the FTIR spectrum of STO are related to the stretching vibrations of Ti-O bonds. These peaks are typically observed in the range of 500–800 cm<sup>-1</sup>. Sr-Ti-O stretching in STO appeared at 580 cm<sup>-1</sup> in both composites as a weak band, which is expected due to a low particle concentration [70,71]. Vibrations from Mn-O are visible at 536 cm<sup>-1</sup> [72].



**Figure 4.** FTIR spectra of PMMA and composites with enlarged region 1500–500  $\text{cm}^{-1}$ .

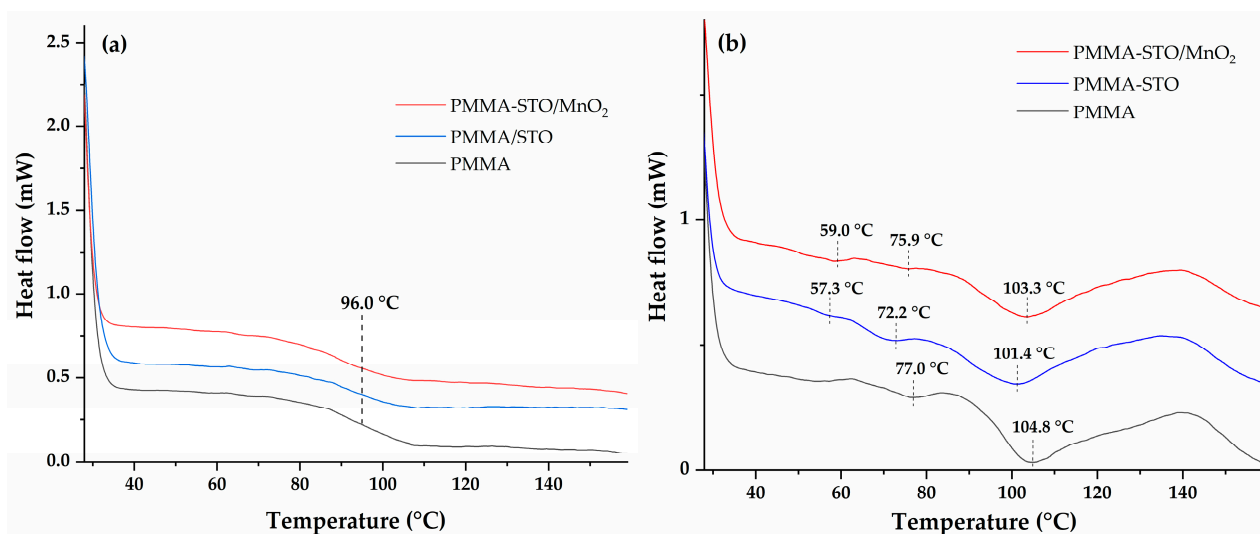
FTIR analysis revealed that hybrid STO/ $\text{MnO}_2$  nanoparticles had a minor influence on influence on polymerization of MMA. The identification of nanoparticles at randomly chosen sites indicates that some level of uniformity was achieved, without the chemical modification of particles.

### 3.5. Differential Scanning Calorimetry (DSC)

Particle agglomeration could lead to deterioration of mechanical properties, acting as stress concentration points that lead to a crack formation. Furthermore, large particles/agglomerates may act as plasticizers, increasing chain mobility and decreasing intermolecular forces that resist applied mechanical force. This is connected to thermal behavior, characterized by glass transition temperature ( $T_g$ ). In order to investigate whether agglomeration lead to a decrease in  $T_g$ , DSC analysis was performed. Figure 5a shows that the formation of nanoparticle agglomerates had no significant influence on  $T_g$ , which is around 96.0 °C in all samples. This finding is indicative and important for the mechanical performance of composites and is in agreement with the literature, where it has been proven that low particle concentrations do not lead to a decrease in composite  $T_g$ .

The first scan presented in Figure 5b shows differences between samples during heating. In PMMA straight baseline was observed until 62.8 °C, where an onset for a weak endothermic peak at 77.0 °C was observed. Another endotherm was observed at 104.8 °C, with an onset at 84.0 °C. On the other side, PMMA-STO/ $\text{MnO}_2$  showed the first endotherm at 59.0 °C, followed by a weak one at 75.9 °C and a strong peak at 103.3 °C. PMMA-STO had a minor endotherm at 57.3 °C, stronger at 72.2 °C, and a major peak at 101.4 °C. The boiling point of MMA is 100 °C, which indicates that in pure PMMA, the monomer was trapped by the polymer chains more efficiently than in composites. Particle agglomerates enabled more mobility for MMA, leading to evaporation at temperatures close to the unhindered monomer. However, these temperature shifts are minor, which leads to the conclusion that there would not be a significant difference in monomer leaching [73]. Furthermore, although other weaker endotherms indicate that volatile additives are easier to release and leach in composites, in PMMA-STO/ $\text{MnO}_2$  there was a weaker endothermic peak compared to PMMA around 76 °C, which indicates that hybrid nanoparticles could more efficiently trap some of the smaller molecules. In light of the results based on thermal analysis, it can be assumed that STO/ $\text{MnO}_2$  agglomerates do not pose a problem from a medical point of view as well.





**Figure 5.** DSC analysis of PMMA and composites: (a) second scan; (b) first scan.

### 3.6. Mechanical Properties

Results obtained from tensile test, microindentation, and controlled energy impact test are presented in Table 1 and Figure 5. Modulus of elasticity increased by 39.6% in PMMA-STO and 44.0% in PMMA-STO/MnO<sub>2</sub>, compared to the pure PMMA. Tensile strength was approximately the same in PMMA-STO and PMMA-STO/MnO<sub>2</sub>, respectively, 29.4% and 29.9% higher than for PMMA. The interface that arises from the bonding between filler particles and polymer chains leads to enhanced mechanical properties in the modified composites compared to the pristine material [74]. Specifically, when STO and STO/MnO<sub>2</sub> nanoparticles were employed to reinforce PMMA, a robust interface ensured that the applied load was transmitted to the resilient inorganic nanoparticles, subsequently distributing it across multiple polymer chains, safeguarding the matrix.

**Table 1.** Mechanical properties of PMMA and composites.

	PMMA	PMMA-STO	PMMA-STO/MnO <sub>2</sub>
Modulus of elasticity, MPa	720.6 ± 22.13	1006.0 ± 15.37	1037.3 ± 24.63
Tensile strength, MPa	23.1 ± 1.22	29.9 ± 1.86	30.0 ± 1.41
Hardness, MPa	14.8 ± 0.43	19.2 ± 1.82	28.1 ± 2.23
E <sub>tot</sub> , J	1.1 ± 0.16	1.9 ± 0.14	2.7 ± 0.21

Microindentation measurements revealed that hardness was increased by 29.7% in PMMA-STO and by 89.9% in PMMA-STO/MnO<sub>2</sub>, which indicates that the small amounts of hybrid STO/MnO<sub>2</sub> nanoparticles can significantly improve mechanical performance. Furthermore, reduced modulus increased by 45.0% in PMMA-STO and by 66.1% in PMMA-STO/MnO<sub>2</sub>. Compared to the studies that investigated the influence of alumina, silica, and zirconia with higher loadings, improvements observed in both composites show great reinforcing potential [26–28]. This phenomenon could be attributed to the considerably higher hardness of the particles in comparison to pure PMMA, thus contributing to an increased load-bearing capacity [32]. The difference in the results between PMMA-STO and PMMA-STO/MnO<sub>2</sub> is a consequence of better STO/MnO<sub>2</sub> dispersion in the matrix, which indicates that MnO<sub>2</sub> contributed to better adhesion between the hybrid particles and the matrix.

The energy absorption process during impact can be divided into distinct phases, as follows [57]:

1. **Initial Crack Formation Phase:** In this first phase, energy is absorbed as the crack initially forms within the material. It encompasses both the elastic response of the

material and any minimal plastic deformation. For fully cured epoxy resins, this phase is characterized by relatively low energy absorption. The maximum load ( $F_{\max}$ ) is achieved at the conclusion of this phase, and the energy absorbed up to this point is denoted as  $E_{f\max}$ .

2. Crack Propagation and Material Deterioration Phase: The second phase commences with the formation of the crack and extends until the material eventually fails or ruptures. During this phase, there is a notable degradation of mechanical properties. The total absorbed energy ( $E_{\text{tot}}$ ) encompasses all the energy absorbed from the start of the controlled energy impact test until the load drops below zero, marking the conclusion of the test.

These phases are associated with different types of failure, depending on the material's propensity for plastic deformation:

- Brittle Failure: This type of failure is characteristic of materials like ceramics and rigid polymer structures, such as cross-linked polymers forming 3D covalently bonded networks. Brittle failure is characterized by minimal or no plastic deformation, rapid fracture propagation, and a low  $E_{\text{tot}}$  value.
- Brittle-Ductile Fracture: In this scenario, there is a limited degree of plastic deformation that occurs just before the material breaks. It represents an intermediate stage between brittle and ductile behaviors.
- Ductile-Brittle Failure: Materials exhibiting this type of failure have the capacity for plastic deformation and can absorb more energy during impact compared to brittle materials. They undergo some plastic deformation before ultimately fracturing.
- Ductile fracture: The fourth type of failure is characterized by substantial plastic deformations occurring before fracture. Materials that exhibit this behavior absorb a significant amount of energy during the impact, resulting in a high  $E_{\text{tot}}$  value.

These distinctions in failure modes and energy absorption characteristics are crucial for understanding how different materials respond to impact loads and for assessing their suitability for various applications. Figure 6 shows failure types for PMMA, PMMA-STO, and PMMA-STO/MnO<sub>2</sub>. PMMA shows brittle failure, which is expected since it is considered a brittle thermoplastic polymer [75]. With the addition of STO, fracture changed to brittle-ductile, which is the consequence of energy dissipation during crack pinning and plastic void formation, observed on FESEM images. In PMMA-STO/MnO<sub>2</sub>, failure mode became ductile-brittle, indicating that STO/MnO<sub>2</sub> have stronger interaction with the matrix, which was indicated in FESEM analysis, where smaller aggregates were observed than in PMMA-STO. However, STO particles led to an increase of 72.7% in  $E_{\text{tot}}$ , which is a significant improvement in impact resistance. Compared to Balguri et al., where a similar amount of pure MnO<sub>2</sub> was used, the increase of 145.4% in total absorbed impact energy achieved in this study shows the remarkable effect of synergy between STO and MnO<sub>2</sub> nanoparticles [49].

In order to verify the statistically significant mechanical improvement, the Student's *t*-test was performed for the results presented in Table 1 [76]. Arithmetic means of control series (PMMA) were compared with PMMA-STO and PMMA-STO/MnO<sub>2</sub>. High *t*- and low *p*-values presented in Table 2 illustrate high statistical significance (threshold:  $t > 1.96$ ,  $p < 0.05$ ) of an increase in all the mechanical properties.

The results obtained from the tensile test, microindentation and controlled energy impact test revealed that there is a high potential for using novel STO/MnO<sub>2</sub> nanoparticles as mechanical reinforcement. Furthermore, these results were obtained without the chemical modification of nanoparticles, which is usually required for significant mechanical improvements [75]. Since both STO and MnO<sub>2</sub> have been already investigated and proven for their biocompatibility and antibacterial activity, the main scope of our future research will be on varying nanoparticle concentration and investigating antibacterial activity.

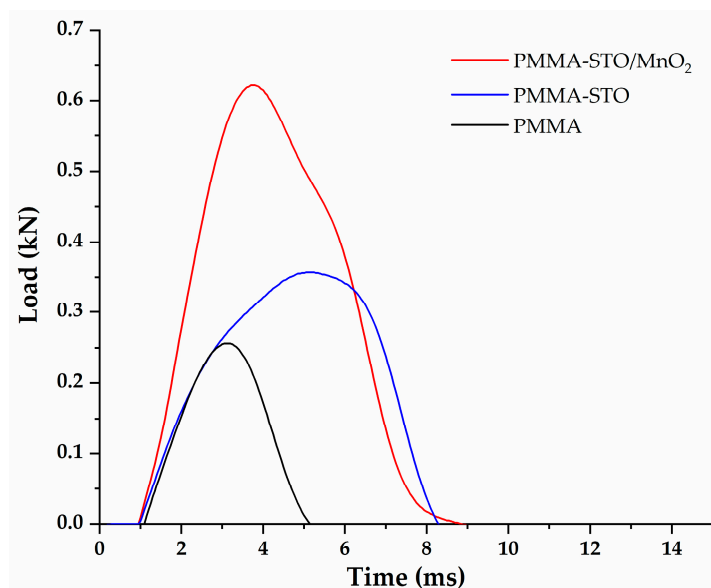


Figure 6. Load-time curves obtained from controlled energy impact test.

Table 2. Results of Student's *t*-test.

	PMMA-STO *		PMMA-STO/MnO <sub>2</sub> ‡	
	t-Value	p-Value	t-Value	p-Value
Modulus of elasticity	18.3465	<0.0001	16.5664	<0.0001
Tensile strength	5.2949	0.0061	6.4097	0.0030
Hardness	4.0752	0.0152	10.1433	0.0005
E <sub>tot</sub>	6.5175	0.0029	10.4970	0.0005

\* Group 1: PMMA, Group 2: PMMA-STO; n (number of measurements) = 3. ‡ Group 1: PMMA, Group 2: PMMA-STO/MnO<sub>2</sub>; n (number of measurements) = 3.

#### 4. Conclusions

In this research, two types of nanoparticulate fillers, STO and hybrid STO/MnO<sub>2</sub>, have been used as reinforcements for dental (PMMA), with the aim of improving its low impact resistance and hardness. Hybrid STO/MnO<sub>2</sub> nanoparticles were obtained by sintering at 1000 °C and incorporating them in the liquid part of the two-component dental PMMA resin, with 1 wt% concentration. Structural analysis of hybrid nanoparticles revealed the existence of cubic STO, as well as  $\beta$ -MnO<sub>2</sub> and  $\gamma$ -MnO<sub>2</sub>. The results of DSC analysis indicated that agglomeration of nanoparticles with a 1 wt% loading had no significant impact on T<sub>g</sub>. However, the first DSC scan revealed disparities in the evaporation of small molecules, with some favoring PMMA-STO/MnO<sub>2</sub> composite that demonstrated a potential for trapping volatiles. Morphological characterization revealed synergy between STO and MnO<sub>2</sub> in STO/MnO<sub>2</sub> nanoparticles, leading to a better dispersion in the matrix, compared to STO. As a consequence of a better dispersion, a higher improvement in PMMA mechanical performance was achieved. In the PMMA-STO composite, microhardness was increased by 29.9%, modulus of elasticity by 39.6%, and total absorbed impact energy (E<sub>tot</sub>) by 72.7%, which showed that even with the formation of aggregates, STO represents a promising reinforcement for PMMA. Composite PMMA-STO/MnO<sub>2</sub> has shown an increase in microhardness by 89.9%, and modulus of elasticity by 44.0%, while E<sub>tot</sub> values rose by 145.4%. These results indicated that a low concentration of novel hybrid STO/MnO<sub>2</sub> nanoparticles could lead to an outstanding mechanical performance by a PMMA-based material.

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## References

1. Rokaya, D.; Srimaneepong, V.; Sapkota, J.; Qin, J.; Siraleartmukul, K.; Siritwongrungron, V. Polymeric Materials and Films in Dentistry: An Overview. *J. Adv. Res.* **2018**, *14*, 25–34. [[CrossRef](#)] [[PubMed](#)]
2. Jiang, X.; Yao, Y.; Tang, W.; Han, D.; Zhang, L.; Zhao, K.; Wang, S.; Meng, Y. Design of Dental Implants at Materials Level: An Overview. *J. Biomed. Mater. Res.* **2020**, *108*, 1634–1661. [[CrossRef](#)] [[PubMed](#)]
3. Özcan, M.; Hotza, D.; Fredel, M.C.; Cruz, A.; Volpato, C.A.M. Materials and Manufacturing Techniques for Polymeric and Ceramic Scaffolds Used in Implant Dentistry. *J. Compos. Sci.* **2021**, *5*, 78. [[CrossRef](#)]
4. Pituru, S.M.; Greabu, M.; Totan, A.; Imre, M.; Pantea, M.; Spinu, T.; Tancu, A.M.C.; Popoviciu, N.O.; Stanescu, I.-I.; Ionescu, E. A Review on the Biocompatibility of PMMA-Based Dental Materials for Interim Prosthetic Restorations with a Glimpse into Their Modern Manufacturing Techniques. *Materials* **2020**, *13*, 2894. [[CrossRef](#)] [[PubMed](#)]
5. Zafar, M.S. Prosthodontic Applications of Polymethyl Methacrylate (PMMA): An Update. *Polymers* **2020**, *12*, 2299. [[CrossRef](#)] [[PubMed](#)]
6. Abad-Coronel, C.; Bravo, M.; Tello, S.; Cornejo, E.; Paredes, Y.; Paltan, C.A.; Fajardo, J.I. Fracture Resistance Comparative Analysis of Milled-Derived vs. 3D-Printed CAD/CAM Materials for Single-Unit Restorations. *Polymers* **2023**, *15*, 3773. [[CrossRef](#)]
7. Kaur, H.; Thakur, A. Applications of Poly(Methyl Methacrylate) Polymer in Dentistry: A Review. *Mater. Today Proc.* **2022**, *50*, 1619–1625. [[CrossRef](#)]
8. Al-Dwairi, Z.N.; Tahboub, K.Y.; Baba, N.Z.; Goodacre, C.J. A Comparison of the Flexural and Impact Strengths and Flexural Modulus of CAD/CAM and Conventional Heat-Cured Polymethyl Methacrylate (PMMA). *J. Prosthodont.* **2020**, *29*, 341–349. [[CrossRef](#)]
9. Karaman, T.; Eser, B.; Altintas, E.; Atala, M.H. Evaluation of the Effects of Finish Line Type and Width on the Fracture Strength of Provisional Crowns. *Odontology* **2021**, *109*, 76–81. [[CrossRef](#)]
10. Alqutaibi, A.Y.; Baik, A.; Almuzaini, S.A.; Farghal, A.E.; Alnazzawi, A.A.; Borzangy, S.; Aboalrejal, A.N.; Abdelaziz, M.H.; Mahmoud, I.I.; Zafar, M.S. Polymeric Denture Base Materials: A Review. *Polymers* **2023**, *15*, 3258. [[CrossRef](#)]
11. Al-Thobity, A.M. The Impact of Polymerization Technique and Glass-Fiber Reinforcement on the Flexural Properties of Denture Base Resin Material. *Eur. J. Dent.* **2020**, *14*, 092–099. [[CrossRef](#)] [[PubMed](#)]
12. Yerliyurt, K.; Taşdelen, T.B.; Eğri, Ö.; Eğri, S. Flexural Properties of Heat-Polymerized PMMA Denture Base Resins Reinforced with Fibers with Different Characteristics. *Polymers* **2023**, *15*, 3211. [[CrossRef](#)]
13. Ali Sabri, B.; Satgunam, M.; Abreeza, N.M.; NAbed, A. A Review on Enhancements of PMMA Denture Base Material with Different Nano-Fillers. *Cogent Eng.* **2021**, *8*, 1875968. [[CrossRef](#)]
14. Díez-Pascual, A.M. PMMA-Based Nanocomposites for Odontology Applications: A State-of-the-Art. *Int. J. Mol. Sci.* **2022**, *23*, 10288. [[CrossRef](#)] [[PubMed](#)]
15. Tham, W.L.; Chow, W.S.; Mohd Ishak, Z.A. Effects of Titanate Coupling Agent on the Mechanical, Thermal, and Morphological Properties of Poly(Methyl Methacrylate)/Hydroxyapatite Denture Base Composites. *J. Compos. Mater.* **2011**, *45*, 2335–2345. [[CrossRef](#)]
16. Sosiati, H.; Rizky, A.M.; Latief, A.L.M.; Adi, R.K.; Hamdan, S. The Mechanical and Physical Properties of Microcrystalline Cellulose (MCC)/Sisal/PMMA Hybrid Composites for Dental Applications. *Mater. Res. Express* **2023**, *10*, 035301. [[CrossRef](#)]
17. Ai, M.; Du, Z.; Zhu, S.; Geng, H.; Zhang, X.; Cai, Q.; Yang, X. Composite Resin Reinforced with Silver Nanoparticles-Laden Hydroxyapatite Nanowires for Dental Application. *Dent. Mater.* **2017**, *33*, 12–22. [[CrossRef](#)]
18. Jiangkongkho, P.; Arksornnukit, M.; Takahashi, H. The Synthesis, Modification, and Application of Nanosilica in Polymethyl Methacrylate Denture Base. *Dent. Mater. J.* **2018**, *37*, 582–591. [[CrossRef](#)]

19. Alhavaz, A.; Rezaei Dastjerdi, M.; Ghasemi, A.; Ghasemi, A.; Alizadeh Sahraei, A. Effect of Untreated Zirconium Oxide Nanofiller on the Flexural Strength and Surface Hardness of Autopolymerized Interim Fixed Restoration Resins. *J. Esthet. Restor. Dent.* **2017**, *29*, 264–269. [[CrossRef](#)]
20. Gad, M.M.; Abualsaud, R. Behavior of PMMA Denture Base Materials Containing Titanium Dioxide Nanoparticles: A Literature Review. *Int. J. Biomater.* **2019**, *2019*, 6190610. [[CrossRef](#)]
21. Malisic, V.; Gajic, V.; Porobic, S.; Pataric, A.; Putic, S.; Vujcic, I. The Effect of Gamma Irradiation on the Synthesis, Microbiological Sterility, and Improvement of Properties of PMMA-Al<sub>2</sub>O<sub>3</sub> Composite Used in Dental Prosthesis Manufacturing. *Radiat. Phys. Chem.* **2023**, *207*, 110846. [[CrossRef](#)]
22. Sharifianjazi, F.; Pakseresht, A.H.; Shahedi Asl, M.; Esmaeilkhani, A.; Nargesi Khoramabadi, H.; Jang, H.W.; Shokouhimehr, M. Hydroxyapatite Consolidated by Zirconia: Applications for Dental Implant. *J. Compos. Compd.* **2020**, *2*, 26–34. [[CrossRef](#)]
23. Passaro, J.; Bifulco, A.; Calabrese, E.; Imparato, C.; Raimondo, M.; Pantani, R.; Aronne, A.; Guadagno, L. Hybrid Hemp Particles as Functional Fillers for the Manufacturing of Hydrophobic and Anti-Icing Epoxy Composite Coatings. *ACS Omega* **2023**, *8*, 23596–23606. [[CrossRef](#)] [[PubMed](#)]
24. Vojdani, M.; Bagheri, R.; Khaledi, A.A.R. Effects of Aluminum Oxide Addition on the Flexural Strength, Surface Hardness, and Roughness of Heat-Polymerized Acrylic Resin. *J. Dent. Sci.* **2012**, *7*, 238–244. [[CrossRef](#)]
25. Hata, K.; Ikeda, H.; Nagamatsu, Y.; Masaki, C.; Hosokawa, R.; Shimizu, H. Dental Poly(Methyl Methacrylate)-Based Resin Containing a Nanoporous Silica Filler. *J. Funct. Biomater.* **2022**, *13*, 32. [[CrossRef](#)]
26. Alhotan, A.; Yates, J.; Zidan, S.; Haider, J.; Silikas, N. Flexural Strength and Hardness of Filler-Reinforced PMMA Targeted for Denture Base Application. *Materials* **2021**, *14*, 2659. [[CrossRef](#)]
27. Gad, M.; Rahoma, A.; Al-Thobity, A.M.; ArRejaie, A. Influence of Incorporation of ZrO<sub>2</sub> Nanoparticles on the Repair Strength of Polymethyl Methacrylate Denture Bases. *Int. J. Nanomed.* **2016**, *11*, 5633–5643. [[CrossRef](#)]
28. Naznin, H.; Mallik, A.K.; Hossain, K.S.; Shahruzzaman, M.; Haque, P.; Rahman, M.M. Enhancement of Thermal and Mechanical Properties of PMMA Composites by Incorporating Mesoporous Micro-Silica and GO. *Results Mater.* **2021**, *11*, 100203. [[CrossRef](#)]
29. Chen, S.-G.; Yang, J.; Jia, Y.-G.; Lu, B.; Ren, L. TiO<sub>2</sub> and PEEK Reinforced 3D Printing PMMA Composite Resin for Dental Denture Base Applications. *Nanomaterials* **2019**, *9*, 1049. [[CrossRef](#)]
30. Alqahtani, M. Mechanical Properties Enhancement of Self-Cured PMMA Reinforced with Zirconia and Boron Nitride Nanopowders for High-Performance Dental Materials. *J. Mech. Behav. Biomed. Mater.* **2020**, *110*, 103937. [[CrossRef](#)]
31. Alqahtani, M. Effect of Hexagonal Boron Nitride Nanopowder Reinforcement and Mixing Methods on Physical and Mechanical Properties of Self-Cured PMMA for Dental Applications. *Materials* **2020**, *13*, 2323. [[CrossRef](#)]
32. Nabhan, A.; Taha, M.; Ghazaly, N.M. Filler Loading Effect of Al<sub>2</sub>O<sub>3</sub>/TiO<sub>2</sub> Nanoparticles on Physical and Mechanical Characteristics of Dental Base Composite (PMMA). *Polym. Test.* **2023**, *117*, 107848. [[CrossRef](#)]
33. Wu, J.; Wang, H.; Mao, L.; Aliha, M.R.M. Composition Optimization of PMMA Base Denture Reinforced with Different Percentages of Nano Hydroxyapatite and Alumina Particles to Obtain Highest K<sub>Ic</sub> and K<sub>IIc</sub> Values Using Hybrid IWO/PSO Algorithm. *Theor. Appl. Fract. Mech.* **2023**, *128*, 104090. [[CrossRef](#)]
34. Beketova, A.; Theocharidou, A.; Tsamesidis, I.; Rigos, A.E.; Pouroutzidou, G.K.; Tzanakakis, E.-G.C.; Kourtidou, D.; Liverani, L.; Ospina, M.A.; Anastasiou, A.; et al. Sol-Gel Synthesis and Characterization of YSZ Nanofillers for Dental Cements at Different Temperatures. *Dent. J.* **2021**, *9*, 128. [[CrossRef](#)] [[PubMed](#)]
35. Kacem, K.; Casanova-Chafer, J.; Ameer, S.; Nsib, M.F.; Llobet, E. Gas Sensing Properties of Graphene Oxide Loaded with SrTiO<sub>3</sub> Nanoparticles. *J. Alloys Compd.* **2023**, *941*, 169011. [[CrossRef](#)]
36. Shi, X.-L.; Wu, H.; Liu, Q.; Zhou, W.; Lu, S.; Shao, Z.; Dargusch, M.; Chen, Z.-G. SrTiO<sub>3</sub>-Based Thermoelectrics: Progress and Challenges. *Nano Energy* **2020**, *78*, 105195. [[CrossRef](#)]
37. Xian, T.; Yang, H.; Di, L.; Ma, J.; Zhang, H.; Dai, J. Photocatalytic Reduction Synthesis of SrTiO<sub>3</sub>-Graphene Nanocomposites and Their Enhanced Photocatalytic Activity. *Nanoscale Res. Lett.* **2014**, *9*, 327. [[CrossRef](#)]
38. Escobar, A.; Muzzio, N.; Angelomé, P.C.; Bordon, A.V.; Martínez, A.; Bindini, E.; Coy, E.; Andreozzi, P.; Grzelczak, M.; Moya, S.E. Strontium Titanate (SrTiO<sub>3</sub>) Mesoporous Coatings for Enhanced Strontium Delivery and Osseointegration on Bone Implants. *Adv. Eng. Mater.* **2019**, *21*, 1801210. [[CrossRef](#)]
39. Sahoo, S.; Sinha, A.; Das, M. Synthesis, Characterization and in Vitro Biocompatibility Study of Strontium Titanate Ceramic: A Potential Biomaterial. *J. Mech. Behav. Biomed. Mater.* **2020**, *102*, 103494. [[CrossRef](#)]
40. Qiao, H.; Zhang, C.; Dang, X.; Yang, H.; Wang, Y.; Chen, Y.; Ma, L.; Han, S.; Lin, H.; Zhang, X.; et al. Gallium Loading into a Polydopamine-Functionalised SrTiO<sub>3</sub> Nanotube with Combined Osteoinductive and Antimicrobial Activities. *Ceram. Int.* **2019**, *45*, 22183–22195. [[CrossRef](#)]
41. Si, Y.; Liu, H.; Yu, H.; Jiang, X.; Sun, D. A Heterogeneous TiO<sub>2</sub>/SrTiO<sub>3</sub> Coating on Titanium Alloy with Excellent Photocatalytic Antibacterial, Osteogenesis and Tribocorrosion Properties. *Surf. Coat. Technol.* **2022**, *431*, 128008. [[CrossRef](#)]
42. Panomsuwan, G.; Takai, O.; Saito, N. Optical and Mechanical Properties of Transparent SrTiO<sub>3</sub> Thin Films Deposited by ECR Ion Beam Sputter Deposition. *Phys. Status Solidi A* **2013**, *210*, 311–319. [[CrossRef](#)]
43. Davoglio, R.A.; Cabello, G.; Marco, J.F.; Biaggio, S.R. Synthesis and Characterization of α-MnO<sub>2</sub> Nanoneedles for Electrochemical Supercapacitors. *Electrochim. Acta* **2018**, *261*, 428–435. [[CrossRef](#)]

44. Mnyipika, S.H.; Munonde, T.S.; Nomngongo, P.N. MnO<sub>2</sub>@Reduced Graphene Oxide Nanocomposite-Based Electrochemical Sensor for the Simultaneous Determination of Trace Cd(II), Zn(II) and Cu(II) in Water Samples. *Membranes* **2021**, *11*, 517. [[CrossRef](#)] [[PubMed](#)]
45. Wang, S.; Zheng, H.; Zhou, L.; Cheng, F.; Liu, Z.; Zhang, H.; Zhang, Q. Injectable Redox and Light Responsive MnO<sub>2</sub> Hybrid Hydrogel for Simultaneous Melanoma Therapy and Multidrug-Resistant Bacteria-Infected Wound Healing. *Biomaterials* **2020**, *260*, 120314. [[CrossRef](#)] [[PubMed](#)]
46. Mallakpour, S.; Abdolmaleki, A.; Tabebordbar, H. Production of PVC/ $\alpha$ -MnO<sub>2</sub>-KH550 Nanocomposite Films: Morphology, Thermal, Mechanical and Pb (II) Adsorption Properties. *Eur. Polym. J.* **2016**, *78*, 141–152. [[CrossRef](#)]
47. Liang, Z.; Wang, H.; Zhang, K.; Ma, G.; Zhu, L.; Zhou, L.; Yan, B. Oxygen-Defective MnO<sub>2</sub>/ZIF-8 Nanorods with Enhanced Antibacterial Activity under Solar Light. *Chem. Eng. J.* **2022**, *428*, 131349. [[CrossRef](#)]
48. Shaheen, S.; Iqbal, A.; Ikram, M.; Ul-Ain, K.; Naz, S.; Ul-Hamid, A.; Shahzadi, A.; Haider, A.; Nabgan, W.; Haider, J. Effective Disposal of Methylene Blue and Bactericidal Benefits of Using GO-Doped MnO<sub>2</sub> Nanorods Synthesized through One-Pot Synthesis. *ACS Omega* **2021**, *6*, 24866–24878. [[CrossRef](#)]
49. Balguri, P.K.; Thumu, U.; DG, H.S.; Penki, T.R.; Chilumala, I. Manganese Dioxide Nanostructures Reinforced Epoxy Nanocomposites: A Study of Mechanical Properties. *Polym.-Plast. Technol. Mater.* **2022**, *61*, 441–460. [[CrossRef](#)]
50. Zhao, Q.; Yang, L.; Chen, K.; Ma, Y.; Peng, Q.; Ji, H.; Qiu, J. Flexible Textured MnO<sub>2</sub> Nanorods/PVDF Hybrid Films with Superior Piezoelectric Performance for Energy Harvesting Application. *Compos. Sci. Technol.* **2020**, *199*, 108330. [[CrossRef](#)]
51. Da Silva, L.F.; Avansi, W.; Moreira, M.L.; Mesquita, A.; Maia, L.J.Q.; Andrés, J.; Longo, E.; Mastelaro, V.R. Relationship between Crystal Shape, Photoluminescence, and Local Structure in SrTiO<sub>3</sub> Synthesized by Microwave-Assisted Hydrothermal Method. *J. Nanomater.* **2012**, *2012*, 890397. [[CrossRef](#)]
52. Le, M.-V.; Vo, N.-Q.-D.; Le, Q.-C.; Tran, V.A.; Phan, T.-Q.-P.; Huang, C.-W.; Nguyen, V.-H. Manipulating the Structure and Characterization of Sr<sub>1-x</sub>LaxTiO<sub>3</sub> Nanocubes toward the Photodegradation of 2-Naphthol under Artificial Solar Light. *Catalysts* **2021**, *11*, 564. [[CrossRef](#)]
53. Abdul-Hameed, A.A.; Othman, F.M.; Fakhri, M.A. Preparation of MgO-MnO<sub>2</sub> Nanocomposite Particles for Cholesterol Sensors. *J. Mater. Sci. Mater. Electron.* **2021**, *32*, 15523–15532. [[CrossRef](#)]
54. Kalubarme, R.S.; Cho, M.-S.; Yun, K.-S.; Kim, T.-S.; Park, C.-J. Catalytic Characteristics of MnO<sub>2</sub> Nanostructures for the O<sub>2</sub> Reduction Process. *Nanotechnology* **2011**, *22*, 395402. [[CrossRef](#)] [[PubMed](#)]
55. Yuan, A.; Wang, X.; Wang, Y.; Hu, J. Textural and Capacitive Characteristics of MnO<sub>2</sub> Nanocrystals Derived from a Novel Solid-Reaction Route. *Electrochim. Acta* **2009**, *54*, 1021–1026. [[CrossRef](#)]
56. Saputra, E.; Muhammad, S.; Sun, H.; Ang, H.-M.; Tadó, M.O.; Wang, S. Manganese Oxides at Different Oxidation States for Heterogeneous Activation of Peroxymonosulfate for Phenol Degradation in Aqueous Solutions. *Appl. Catal. B Environ.* **2013**, *142–143*, 729–735. [[CrossRef](#)]
57. Qu, D. The Study of the Proton Diffusion Process in the Porous MnO<sub>2</sub> Electrode. *Electrochim. Acta* **2004**, *49*, 657–665. [[CrossRef](#)]
58. Lu, P.; Hu, X.; Li, Y.; Zhang, M.; Liu, X.; He, Y.; Dong, F.; Fub, M.; Zhang, Z. One-step preparation of a novel SrCO<sub>3</sub>/g-C<sub>3</sub>N<sub>4</sub> nano-composite and its application in selective adsorption of crystal violet. *RSC Adv.* **2018**, *8*, 6315. [[CrossRef](#)]
59. Shokrieh, M.M.; Ghoreishi, S.M.; Esmkhani, M. Toughening Mechanisms of Nanoparticle-Reinforced Polymers. In *Toughening Mechanisms in Composite Materials*; Elsevier: Amsterdam, The Netherlands, 2015; pp. 295–320, ISBN 978-1-78242-279-2.
60. Demirci, M.T.; Tarakçoğlu, N.; Avcı, A.; Akdemir, A.; Demirci, İ. Fracture Toughness (Mode I) Characterization of SiO<sub>2</sub> Nanoparticle Filled Basalt/Epoxy Filament Wound Composite Ring with Split-Disk Test Method. *Compos. Part B Eng.* **2017**, *119*, 114–124. [[CrossRef](#)]
61. Tian, K.V.; Yang, B.; Yue, Y.; Bowron, D.T.; Mayers, J.; Donnan, R.S.; Dobó-Nagy, C.; Nicholson, J.W.; Fang, D.-C.; Greer, A.L.; et al. Atomic and Vibrational Origins of Mechanical Toughness in Bioactive Cement during Setting. *Nat. Commun.* **2015**, *6*, 8631. [[CrossRef](#)]
62. Stajic, I.; Veljkovic, F.; Petrovic, M.; Veličkovic, S.; Radojevic, V.; Vlahović, B.; Stajic, A. Impact- and Thermal-Resistant Epoxy Resin Toughened with Acacia Honey. *Polymers* **2023**, *15*, 2261. [[CrossRef](#)] [[PubMed](#)]
63. Quaresimin, M.; Salviato, M.; Zappalorto, M. Toughening Mechanisms in Nanoparticle Polymer Composites. In *Toughening Mechanisms in Composite Materials*; Elsevier: Amsterdam, The Netherlands, 2015; pp. 113–133, ISBN 978-1-78242-279-2.
64. Rahmani, H.; Eslami-Farsani, R.; Ebrahimzhad-Khaljiri, H. High Velocity Impact Response of Aluminum- Carbon Fibers-Epoxy Laminated Composites Toughened by Nano Silica and Zirconia. *Fibers Polym.* **2020**, *21*, 170–178. [[CrossRef](#)]
65. Yousefi, F.; Mousavi, S.B.; Heris, S.Z.; Naghash-Hamed, S. UV-Shielding Properties of a Cost-Effective Hybrid PMMA-Based Thin Film Coatings Using TiO<sub>2</sub> and ZnO Nanoparticles: A Comprehensive Evaluation. *Sci. Rep.* **2023**, *13*, 7116. [[CrossRef](#)] [[PubMed](#)]
66. Abozaid, R.M.; Lazarević, Z.Ž.; Radović, I.; Gilić, M.; Šević, D.; Rabasović, M.S.; Radojević, V. Optical Properties and Fluorescence of Quantum Dots CdSe/ZnS-PMMA Composite Films with Interface Modifications. *Opt. Mater.* **2019**, *92*, 405–410. [[CrossRef](#)]
67. Ramesh, S.; Leen, K.H.; Kumutha, K.; Arof, A.K. FTIR Studies of PVC/PMMA Blend Based Polymer Electrolytes. *Spectrochim. Acta Part A Mol. Biomol. Spectrosc.* **2007**, *66*, 1237–1242. [[CrossRef](#)] [[PubMed](#)]
68. Tripathi, S.N.; Saini, P.; Gupta, D.; Choudhary, V. Electrical and Mechanical Properties of PMMA/Reduced Graphene Oxide Nanocomposites Prepared via in Situ Polymerization. *J. Mater. Sci.* **2013**, *48*, 6223–6232. [[CrossRef](#)]
69. ElFaham, M.M.; Mostafa, A.M.; Nasr, G.M. Unmanned Aerial Vehicle (UAV) Manufacturing Materials: Synthesis, Spectroscopic Characterization and Dynamic Mechanical Analysis (DMA). *J. Mol. Struct.* **2020**, *1201*, 127211. [[CrossRef](#)]

70. Youssef, A.M.; Farag, H.K.; El-Kheshen, A.; Hammad, F.F. Synthesis of Nano-Structured Strontium Titanate by Sol-Gel and Solid State Routes. *Silicon* **2018**, *10*, 1225–1230. [[CrossRef](#)]
71. Xie, T.; Wang, Y.; Liu, C.; Xu, L. New Insights into Sensitization Mechanism of the Doped Ce (IV) into Strontium Titanate. *Materials* **2018**, *11*, 646. [[CrossRef](#)]
72. Kumar, Y.; Chopra, S.; Gupta, A.; Kumar, Y.; Uke, S.J.; Mardikar, S.P. Low temperature synthesis of MnO<sub>2</sub> nanostructures for supercapacitor application. *Mater. Sci. Energy Technol.* **2020**, *3*, 566–574. [[CrossRef](#)]
73. Alla, R.; Raghavendra, K.; Vyas, R.; Konakanchi, A. Conventional and contemporary polymers for the fabrication of denture prosthesis: Part I—overview, composition and properties. *Int. J. Appl. Dent. Sci.* **2015**, *1*, 82–89.
74. Chrysafi, I.; Kontonasaki, E.; Anastasiou, A.D.; Patsiaoura, D.; Papadopoulou, L.; Vourlias, G.; Vouvoudi, E.; Bikiaris, D. Mechanical and Thermal Properties of PMMA Resin Composites for Interim Fixed Prostheses Reinforced with Calcium  $\beta$ -Pyrophosphate. *J. Mech. Behav. Biomed. Mater.* **2020**, *112*, 104094. [[CrossRef](#)] [[PubMed](#)]
75. Elmadani, A.A.; Radović, I.; Tomić, N.Z.; Petrović, M.; Stojanović, D.B.; Heinemann, R.J.; Radojević, V. Hybrid Denture Acrylic Composites with Nanozirconia and Electrospun Polystyrene Fibers. *PLoS ONE* **2019**, *14*, e0226528. [[CrossRef](#)] [[PubMed](#)]
76. Gauthier, T.D.; Hawley, M.E. Chapter 5—Statistical Methods. In *Introduction to Environmental Forensics*, 2nd ed.; Academic Press: New York, NY, USA, 2007; pp. 129–183, ISBN 9780123695222. [[CrossRef](#)]

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